

**HELICAL NEEDLE APPARATUS FOR CREATING A  
VIRTUAL ELECTRODE USED FOR THE ABLATION OF TISSUE**

This application claims the benefit of U.S. Provisional Application No. 60/091,969,  
5 filed on July 7, 1998.

**Field of the Invention**

The present invention relates generally to an apparatus for creating a virtual electrode.  
More particularly, the present invention relates to an apparatus for the creation of a virtual  
10 electrode that is useful for the ablation of soft tissue and neoplasms.

**Background of the Present Invention**

The utilization of an electric current to produce an ameliorative effect on a bodily  
tissue has a long history, reportedly extending back to the ancient Greeks. The effects on  
15 bodily tissue from an applied electric current, and thus the dividing line between harmful and  
curative effects, will vary depending upon the voltage levels, current levels, the length of  
time the current is applied, and the tissue involved. One such effect resulting from the  
passage of an electric current through tissue is heat generation.

Body tissue, like all non-superconducting materials, conducts current with some  
20 degree of resistance. This resistance creates localized heating of the tissue through which the  
current is being conducted. The amount of heat generated will vary with the power  $P$   
deposited in the tissue, which is a function of the product of the square of the current  $I$  and  
the resistance  $R$  of the tissue to the passage of the current through it ( $P = I^2R$ ).

As current is applied to tissue, then, heat is generated due to the inherent resistance of  
25 the tissue. Deleterious effects in the cells making up the tissue begin to occur at about 42°  
Celsius. As the temperature of the tissue increases due to heat generated by the tissue's  
resistance, the tissue will undergo profound changes and eventually, as the temperature  
becomes high enough, that is, generally greater than 45° C, the cells will die. The zone of  
cell death is known as a lesion and the procedure followed to create the lesion is commonly  
30 called an ablation. As the temperature increases beyond cell death temperature, complete  
disintegration of the cell walls and cells caused by boiling off of the tissue's water can occur.

Cell death temperatures can vary somewhat with the type of tissue to which the power is being applied, but generally will begin to occur within the range of 45° to 60° C, though actual cell death of certain tissue cells may occur at a higher temperature.

In recent times, electric current has found advantageous use in surgery, with the development of a variety of surgical instruments for cutting tissue or for coagulating blood. Still more recently, the use of alternating electric current to ablate, that is, kill, various tissues has been explored. Typically, current having a frequency from about 3 kilohertz to about 300 gigahertz, which is generally known as radiofrequency or radiofrequency (RF) current, is used for this procedure. Destruction, that is, killing, of tissue using an RF current is commonly known as radiofrequency ablation. Often radiofrequency ablation is performed as a minimally invasive procedure and is thus known as radiofrequency catheter ablation because the procedure is performed through and with the use of a catheter. By way of example, radiofrequency catheter ablation has been used to ablate cardiac tissue responsible for irregular heart beats or arrhythmias.

The prior art applications of current to tissue have typically involved applying the current using a "dry" electrode. That is, a metal electrode is applied to the tissue desired to be affected and a generated electric current is passed through the electrode to the tissue. A commonly known example of an instrument having such an operating characteristic is an electrosurgical instrument known as a "bovie" knife. This instrument includes a cutting/coagulating blade electrically attached to a current generator. The blade is applied to the tissue of a patient and the current passes through the blade into the tissue and through the patient's body to a metal base electrode or ground plate usually placed underneath and in electrical contact with the patient. The base electrode is in turn electrically connected to the current generator so as to provide a complete circuit.

As the current from the bovie knife passes from the blade into the tissue, the resistance provided by the tissue creates heat. In the cutting mode, a sufficient application of power through the bovie knife to the tissue causes the fluid within the cell to turn to steam, creating a sufficient overpressure so as to burst the cell walls. The cells then dry up, desiccate, and carbonize, resulting in localized shrinking and an opening in the tissue.

Alternatively, the bovie knife can be applied to bleeding vessels to heat and coagulate the blood flowing therefrom and thus stop the bleeding.

As previously noted, another use for electrical instruments in the treatment of the body is in the ablation of tissue. To expand further on the brief description given earlier of the ablation of cardiac tissue, it has long been known that a certain kind of heart tissue known as sino-atrial and atrio-ventricular nodes spontaneously generate an electrical signal that is propagated throughout the heart along conductive pathways to cause it to beat. Occasionally, certain heart tissue will "misfire," causing the heart to beat irregularly. If the errant electrical pathways can be determined, the tissue pathways can be ablated and the irregular heartbeat remedied. In such a procedure, an electrode is placed via a catheter into contact with the tissue and then current is applied to the tissue via the electrode from a generator of RF current. The applied current will cause the tissue in contact with the electrode to heat. Power will continue to be applied until the tissue reaches a temperature where the heart tissue dies, thereby destroying the errant electrical pathway and the cause of the irregular heartbeat.

Another procedure using RF ablation is transurethral needle ablation, or TUNA, which is used to create a lesion in the prostate gland for the treatment of benign prostatic hypertrophy (BPH) or the enlargement of the prostate gland. In a TUNA procedure, a needle having an exposed conductive tip is inserted into the prostate gland and current is applied to the prostate gland via the needle. As noted previously, the tissue of the prostate gland heats locally surrounding the needle tip as the current passes from the needle to the base electrode. A lesion is created as the tissue heats and the destroyed cells may be reabsorbed by the body, infiltrated with scar tissue, or just become non-functional.

While there are advantages and uses for such "dry" electrode instruments, there are also several notable disadvantages. One of these disadvantages is that during a procedure, coagulum--dried blood cells and tissue cells--will form on the electrode engaging the tissue. Coagulum acts as an insulator and effectively functions to prevent current transfer from the blade to the tissue. This coagulum "insulation" can be overcome with more voltage so as to keep the current flowing, but only at the risk of arcing and injuring the patient. Thus, during surgery when the tissue is cut with an electrosurgical scalpel, a build-up of coagulated blood

and desiccated tissue will occur on the blade, requiring the blade to be cleaned before further use. Typically, cleaning an electrode/scalpel used in this manner will involve simply scraping the dried tissue from the electrode/scalpel by rubbing the scalpel across an abrasive pad to remove the coagulum. This is a tedious procedure for the surgeon and the operating  
5 staff since it requires the "real" work of the surgery to be discontinued while the cleaning operation occurs. This procedure can be avoided with the use of specially coated blades that resist the build up of coagulum. Such specialty blades are costly, however.

A second disadvantage of the dry electrode approach is that the electrical heating of the tissue creates smoke that is now known to include cancer-causing agents. Thus, preferred  
10 uses of such equipment will include appropriate ventilation systems, which can themselves become quite elaborate and quite expensive.

A further, and perhaps the most significant, disadvantage of dry electrode  
15 electrosurgical tools is revealed during cardiac ablation procedures. During such a procedure, an electrode that is otherwise insulated but having an exposed, current carrying tip is inserted into the heart chamber and brought into contact with the inner or endocardial side of the heart wall where the ablation is to occur. The current is initiated and passes from the current generator to the needle tip electrode and from there into the tissue so that a lesion is created. Typically, however, the lesion created by a single insertion is insufficient to cure the irregular  
20 heartbeat because the lesion created is of an insufficient size to destroy the errant electrical pathway. Thus, multiple needle insertions and multiple current applications are almost always required to ablate the errant cardiac pathway, prolonging the surgery and thus increasing the potential risk to the patient.

This foregoing problem is also present in TUNA procedures, which similarly require  
25 multiple insertions of the needle electrode into the prostate gland. Failing to do so will result in the failure to create a lesion of sufficient size otherwise required for beneficial results. As with radiofrequency catheter ablation of cardiac tissue, then, the ability to create a lesion of the necessary size to alleviate BPH symptoms is limited and thus requires multiple insertions of the electrode into the prostate.

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5 A typical lesion created with a dry electrode using RF current and a single insertion will normally not exceed one centimeter in diameter. This small size--often too small to be of much or any therapeutic benefit--stems from the fact that the tissue surrounding the needle electrode tends to desiccate as the temperature of the tissue increases, leading to the creation of a high resistance to the further passage of current from the needle electrode into the tissue, all as previously noted with regard to the formation of coagulum on an electrosurgical scalpel. This high resistance—more properly termed impedance since typically an alternating current is being used—between the needle electrode and the base electrode is commonly measured by the RF current generator. When the measured impedance reaches a pre-

10 determined level, some prior art generators will discontinue current generation. Discontinuance of the ablation procedure under these circumstances is necessary to avoid injury to the patient.

15 Thus, a typical procedure with a dry electrode may involve placing the needle electrode at a first desired location; energizing the electrode to ablate the tissue; continue applying current until the generator measures a high impedance and shuts down; moving the needle to a new location closely adjacent to the first location; and applying current again to the tissue through the needle electrode. This cycle of electrode placement, electrode energization, generator shut down, electrode re-emplacment, and electrode re-energization, will be continued until a lesion of the desired size has been created. As noted, this increases the length of the procedure for the patient. Additionally, multiple insertions increases the risk of at least one of the placements being in the wrong location and, consequently, the risk that healthy tissue may be undesirably affected while diseased tissue may be left untreated. The traditional RF ablation procedure of using a dry ablation therefore includes several patient risk factors that both patient and physician would prefer to reduce or eliminate.

25 The therapeutic advantages of RF current could be increased if a larger lesion could be created safely with a single positioning of the current-supplying electrode. A single positioning would allow the procedure to be carried out more expeditiously and more efficiently, reducing the time involved in the procedure. Larger lesions can be created in at least two ways. First, simply continuing to apply current to the patient with sufficiently

increasing voltage to overcome the impedance rises will create a larger lesion, though almost always with undesirable results to the patient. Second, a larger lesion can be created if the current density, that is, the applied electrical energy, could be spread more efficiently throughout a larger volume of tissue. Spreading the current density over a larger tissue  
5 volume would correspondingly cause a larger volume of tissue to heat in the first instance. That is, by spreading the applied power throughout a larger tissue volume, the tissue would heat more uniformly over a larger volume, which would help to reduce the likelihood of generator shutdown due to high impedance conditions. The applied power, then, will cause the larger volume of tissue to be ablated safely, efficiently, and quickly.

10 Research conducted under the auspices of the assignee of the present invention has focused on spreading the current density throughout a larger tissue volume through the creation, maintenance, and control of a "virtual electrode" within or adjacent to the tissue to be ablated. A virtual electrode can be created by the introduction of a conductive fluid, such as isotonic or hypertonic saline, into or onto the tissue to be ablated. The conductive fluid  
15 will facilitate the spread of the current density substantially equally throughout the extent of the flow of the conductive fluid, thus creating an electrode--a virtual electrode--substantially equal in extent to the size of the delivered conductive fluid. RF current can then be passed through the virtual electrode into the tissue.

A virtual electrode can be substantially larger in volume than the needle tip electrode  
20 typically used in RF interstitial ablation procedures and thus can create a larger lesion than can a dry, needle tip electrode. That is, the virtual electrode spreads or conducts the RF current density outward from the RF current source—such as a current carrying needle, forceps or other current delivery device—into or onto a larger volume of tissue than is possible with instruments that rely on the use of a dry electrode. Stated otherwise, the  
25 creation of the virtual electrode enables the current to flow with reduced resistance or impedance throughout a larger volume of tissue, thus spreading the resistive heating created by the current flow through a larger volume of tissue and thereby creating a larger lesion than could otherwise be created with a dry electrode.

While the efficacy of RF current ablation techniques using a virtual electrode has been demonstrated in several studies, the currently available instruments useful in such procedures lags behind the research into and development of hoped-for useful treatment modalities for the ablation of soft tissue and malignancies.

5 It would be desirable to have an apparatus capable of creating a virtual electrode for the controlled application of tissue ablating RF electric current to a tissue of interest so as to produce a lesion of desired size and configuration.

### **Summary of the Invention**

10 One aspect of the present invention provides a surgical apparatus for delivering conductive fluid to a target site for subsequent formation of a virtual electrode to ablate bodily tissue at the target site by applying a current to the delivered conductive fluid. The surgical apparatus comprises an elongated device forming a helical needle assembly. The helical needle assembly includes a helical needle configured to engage bodily tissue. The  
15 helical needle is hollow for delivering conductive fluid from a fluid source and forms a needle tip. In one preferred embodiment, an electrode is associated with the helical needle assembly for applying a current to conductive fluid delivered from the helical needle assembly. During use, the helical needle assembly is maneuvered into contact with bodily tissue at a desired location. Conductive fluid is delivered to the tissue via the hollow helical  
20 needle. The electrode applies a current to the so-delivered conductive fluid, thereby creating a virtual electrode for ablating the bodily tissue.

Another aspect of the present invention relates to a surgical system for creating a virtual electrode to ablate bodily tissue. The system includes a fluid source, a current source and a surgical instrument. The fluid source maintains a supply of conductive fluid. The  
25 current source is configured to selectively supply a current. Finally, the surgical instrument includes an elongated device forming a helical needle and an electrode associated with the helical needle. The helical needle is configured to engage bodily tissue. Further, the helical needle is hollow and is fluidly connected to the fluid source for delivering the conductive fluid. Finally, the helical needle terminates in a needle tip. The electrode is associated with

the helical needle and is connected to the current source. With this configuration, during use, the helical needle is maneuvered into engagement with a desired location of bodily tissue. Conductive fluid is delivered to the bodily tissue via the helical needle. The current source is then activated to supply a current to the electrode, in turn applying a current to the conductive fluid delivered from the helical needle. Application of the current to the delivered conductive fluid creates a virtual electrode, thereby ablating bodily tissue in contact therewith.

### **Brief Description of the Drawings**

FIG. 1 is a block diagram of a surgical system for creating a virtual electrode to ablate bodily tissue in accordance with the present invention;

FIG. 2 is an enlarged, side view of a helical needle portion of a surgical instrument used with the system of FIG. 1;

FIG. 3 is a side view of an alternative helical needle in accordance with the present invention;

FIG. 4 is an enlarged, side view of an alternative helical needle in accordance with the present invention;

FIG. 5 is an enlarged, side view of an alternative helical needle in accordance with the present invention;

FIG. 6 is an enlarged, side view of an alternative helical needle in accordance with the present invention;

FIG. 7 is an enlarged, exploded view of an alternative helical needle assembly in accordance with the present invention;

FIG. 8 is an enlarged, side view of an alternative helical needle assembly in accordance with the present invention;

FIG. 9 is an enlarged, side view of an alternative helical needle assembly in accordance with the present invention;

FIG. 10 is an enlarged, perspective view of an alternative helical needle in accordance with the present invention;



FIG. 11 is an enlarged, perspective view of an alternative helical needle assembly in accordance with the present invention;

FIG. 12 is an enlarged, cross-sectional view of an alternative helical needle in accordance with the present invention;

5 FIG. 13 is an enlarged, side view of an alternative helical needle in accordance with the present invention;

FIG. 14 is an enlarged, cross-sectional view of an alternative helical needle in accordance with the present invention; and

10 FIG. 15 is an enlarged, perspective view of an alternative helical needle assembly in accordance with the present invention.

### **Detailed Description of the Present Invention**

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15 Figure 1 illustrates in block form a surgical system 20 for RF ablation useful with the present invention. The surgical system 20 includes a current source of radiofrequency alternating electric current 22, a fluid source of RF ablating fluid 24, including but not limited to saline and other conductive solutions, and a surgical instrument 26 for delivering the RF current and the ablation fluid to a tissue site (not shown) for ablation purposes. In one preferred embodiment, the surgical instrument 26 is connected to the current source 22 and the fluid source 24. It will be understood that the current source 22 and the fluid source 24  
20 may be combined into a single operational structure controlled by an appropriate microprocessor for a controlled delivery of ablating fluid and a controlled application of RF current, both based upon measured parameters such as but not limited to, flow rate, tissue temperature at the ablation site and at areas surrounding the ablation site, impedance, the rate of change of the impedance, the detection of arcing between the surgical instrument and the  
25 tissue, the time period during which the ablation procedure has been operating, and additional factors as desired.

While the surgical instrument 26 is shown as being connected to both the current source 22 and the fluid source 24, the present system is not so limited but could include separate instruments for those purposes. For example, a separate needle or similar apparatus

could be used to deliver the current and a separate needle or needles could be used to deliver fluid to the target tissue. In addition, the application of the surgical system 20 illustrated in FIG. 1 is not limited to the use of straight needles or helical needles as surgical instruments but could find use with any type of instrument wherein a conductive solution is delivered to a tissue and an RF current is applied to the tissue through the conductive fluid. Such instruments thus would include straight needles, helical needles, forceps, roller balls, or other instruments for the treatment of vascular disorders, and any other instrument.

As described above, the surgical instrument 26 may assume a wide variety of forms. In accordance with the present invention, however, the surgical instrument includes an elongated device terminating in a helical needle assembly configured to deliver the conductive fluid as well as to apply a current to the so-delivered fluid. Various embodiments of acceptable helical needle configurations are shown in FIGS. 2-15. For example, FIG. 2 illustrates one embodiment of a helical needle or helical needle assembly 30. The helical needle 30 is preferably hollow, terminating in a needle tip 32 at a distal end 34 thereof. The needle tip 32 defines an opening (not shown) for delivering conductive fluid supplied to the helical needle via the fluid source 24 (FIG. 1). Further, as previously described, the helical needle 30 is preferably configured to serve as an electrode for applying a current, via the current source 22 (FIG. 1), to the delivered conductive fluid. With the above in mind, the helical needle defines a pitch P between adjacent coils 36 that increases in the distal direction. This varying pitch facilitates first the engagement of the needle tip 32 with tissue (not shown) at a target site and its initial threading therein. As the pitch between adjacent coils 36 of the helical needle 30 decreases in the proximal direction, the adjacent coils 36 more tightly engage the tissue, thereby providing a better seal between the tissue and the needle coils 36. This greater sealing ability reduces the likelihood that the conductive fluid, which is heated during the ablation process to a temperature capable of killing cells, will not leak back along the track in the tissue made by the helical needle 30. Thus, the conductive solution will tend to stay closely adjacent to the needle tip 32 rather than leak backwards along the needle track and unintentionally and undesirably damage or destroy other healthy tissue.

Referring now to FIGS. 3 and 4, alternative embodiments of a fluid and RF current delivery helical needle 40 and 50 are illustrated. Both helical needles 40 and 50 are hollow, terminating in a needle tip 42, 52, respectively, and have a variable diameter that changes in the proximal to distal direction. In the case of the helical needle 40, an outer diameter of the helical needle 40 increases in the proximal to distal direction, whereas with the helical needle 50, the outer diameter decreases in the proximal to distal direction. Varying the diameter in this manner may allow for better sealing of the tissue (not shown) in the affected region against the coils comprising the respective helical needle 40 or 50. That is, alternating the diameter in the manner shown increases the loading of the tissue across the various coils unlike a uniformly coiled needle, wherein the tissue loading is uniform across the coils. Varying the diameter will also affect the amount of torque that must be applied by a surgeon to screw the needle tip 42, 52 into the tissue to be ablated. Thus, with respect to the helical needle 40, as the helical needle 40 is turned into the tissue, the torque necessary to rotate the needle tip 42 increases because the coils force the engaged tissue into a smaller diameter, thus substantially sealing a resulting needle track against leakage of heated conductive fluid there along. Similarly, with respect to the helical needle 50 as shown in FIG. 4, the helical needle 50 first engages a relatively small portion of tissue and subsequently forces the larger diameter coils into the same needle track as followed by the initially small diameter needle tip 52.

Referring now to FIG. 5, an alternate embodiment of helical needle 60 useful in an RF ablation procedure is shown. As with previous embodiments, the helical needle 60 is hollow to provide a flow path for conductive fluid, and defines a needle tip 62 through which the conductive fluid exits the helical needle 60. Additionally, the helical needle 60 has a diameter that first increases in the proximal to distal direction and then decreases to a diameter somewhat similar to the initial coil diameter at the needle tip 62.

Yet another alternative embodiment of a helical needle 70 is shown in FIG. 6. The helical needle 70 has a coil diameter that decreases in the proximal to distal direction for a predefined predetermined distance and then increases to a diameter substantially equal to the original diameter. Once again, the helical needle 70 is hollow and has a needle tip 72

defining an opening for the outflow of conductive fluid. Both of the embodiments 60 and 70 shown in FIGS. 5 and 6 provide for a varying torque and increased sealing ability due to the action of the helical needle 60 and 70 forcing the tissue (not shown) to follow the coils through the tissue as the diameter thereof varies.

5 Yet another alternate embodiment of a helical needle assembly 80 is shown in exploded view in FIG. 7. The helical needle assembly 80 comprises a plurality of concentric helical needles 82, 84 and 86. Alternatively, only two such helical needles could be provided or additional helical needles may be used as desired. The use of a plurality of concentrically disposed helical needles 82, 84 and 86 allows the physician to engage thinner tissues (not  
10 shown), such as the atrial wall. The concentric helical needles 82, 84 and 86 are preferably wound in the same direction to facilitate insertion and capture of the tissue. Each helical needle 82, 84 and 86 includes a needle tip 83, 85 and 87, respectively. As desired, the helical needles 82, 84 and 86 are hollow to provide a fluid path for conductive fluid from the fluid source 24 (FIG. 1) with the fluid exiting through needle tips 83, 85 and 87 respectively. That  
15 is, one or more of the helical needles 82, 84 or 86 could be used to provide fluid to the tissue to be ablated. Additionally, one or more of the helical needles 82, 84 or 86 may be used as a suction path for removal of conductive fluid.

Yet another alternative embodiment of a helical needle assembly 90 is depicted in FIG. 8. In general terms, the helical needle assembly 90 comprises a plurality of helical  
20 needles, here 92 and 94, wound parallel to one another. As with previous embodiments, each of the helical needles 92 and 94 are preferably hollow, terminating in an open, needle tip 96 and 98, respectively. The use of a parallel assembly would enable the physician performing an ablation procedure to use one of the helical needles 92 or 94 as a fluid path for providing conductive fluid from the fluid source 24 (FIG. 1) to the tissue (not shown) to be ablated and  
25 the second helical needle 92 or 94 as a vacuum source for removal of the conductive fluid. The use of suction to remove the ablation fluid either during or at the end of the procedure will reduce the likelihood of leakage of the hot conductive fluid backwards along the needle track.

Yet another alternative embodiment of a helical needle assembly 100 is shown in FIG. 9. The helical needle assembly 100 is similar to the helical needle assembly 80 (FIG. 7) previously described. The helical needle assembly 100 includes outer and inner helical needles 102 and 104 concentrically arranged. As with the embodiment shown in FIG. 7, the concentric helical needles 102, 104 may be used to deliver fluid at different depths in a tissue (not shown) or one or more flow paths could be used to provide suction and removal of the ablating solution from the tissue during or subsequent to the termination of the application of RF power to the tissue, via the current source 22 (FIG. 1). As shown in FIG. 9, only two such concentric helical needles 102, 104 are shown, though multiple coils in excess of two could be used.

It will be understood that the various configurations could be combined in several of the embodiments shown. For example, the variable pitch shown in FIG. 2 could be combined with the variable diameters shown in FIGS. 3-5 and 8. In addition, the variable diameter structure shown in FIGS. 3-6 could be combined with the parallel assembly construction shown in FIG. 8.

Referring now to FIGS. 10 and 11, alternate embodiments of helical needle assemblies 110 and 120, including alternate means of anchoring a needle to a tissue (not shown), are shown. With reference to FIG. 10, the helical needle assembly 110 is an archimedes type screw comprising a central shaft 112 about which a helical flight 114 is wound. The central shaft 112 is preferably hollow for delivering conductive fluid from the fluid source 24 (FIG. 1). The helical needle assembly 120 has a substantially straight fluid and current delivery portion 122 mounted substantially centrally of a disc 124 having a plurality of starting threads 126. The starting threads 126 will engage the tissue (not shown), such as a cardiac wall, and will anchor the helical needle assembly 120 thereto. Though it be understood that the straight needle portion 122 would penetrate the tissue wall to deliver fluid and electric current from the fluid source 24 (FIG. 1) and the current source 22 (FIG. 1), respectively.

In the discussion of FIGS. 2-11, it has been understood that each embodiment described would deliver conductive fluid through a single aperture at the needle tip. The

present invention is not so limited however. Thus, the fluid could be delivered to the tissue (not shown) by laser drilling a plurality of holes along the length of the various coiled needle configurations. These laser drilled fluid delivery apertures could be configured as desired in terms of size and well as number and distance from each other along the longitudinal extent of the helical needle. FIGS. 12-14 illustrate yet additional fluid delivery methods. Thus, as shown at FIG. 12, a helical needle 130 could include openings 132 extending along part of an outer diameter of the helical needle 130. Alternatively, a helical needle 140 is shown in FIG. 13 as including an open slit 142 extending along an outer diameter thereof. Conversely, a helical needle 150 is depicted in FIG. 14 as having a coil structure wherein a fluid delivery aperture or slit 152 extends along the inner diameter of the needle coils.

FIG. 15 illustrates yet another alternative embodiment of a helical needle assembly 160 in accordance with the present invention including a pair of concentric helical needles 162 and 164. The first helical needle 162 is a large diameter needle whose end 166 (shown partially) is used to anchor the instrument in tissue 168. The second helical needle 164 has a smaller diameter than the first helical needle 162 and is disposed substantially coaxially therewith. Each of the helical needles 162 and 164 may include a hollow interior to provide a flow path for conductive fluid from the fluid source 24 (FIG. 1) and each could be electrically active, via the current source 22 (FIG. 1), through known appropriate connections. Either or both of the helical needles 162, 164 may be used to deliver conductive fluid and either of the helical needles 162, 164 could be electrically active. Alternatively, the helical needles 162 and 164 could form a bipolar needle wherein the helical needles 162, 164 have opposing polarities and the current provided by one travels to the other.

Although the present invention has been described with reference to preferred embodiments, workers skilled in the art will recognize that changes may be made in form and detail without departing from the spirit and scope of the invention.